

Studies on silica and metallic nanoparticles and their possible use for bio-medical applications



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BIOMEDICAL ACTIVITIES AT RRCAT

Use of light (lasers) for

➤ Biomedical Imaging

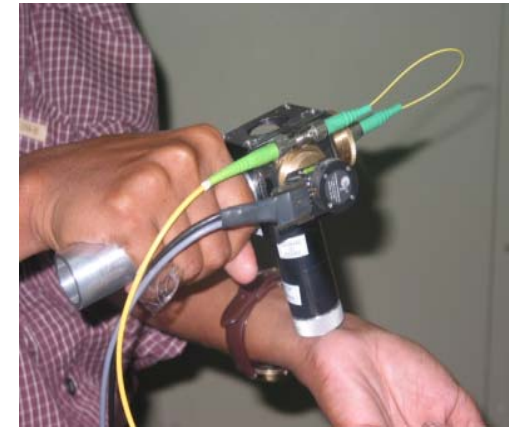
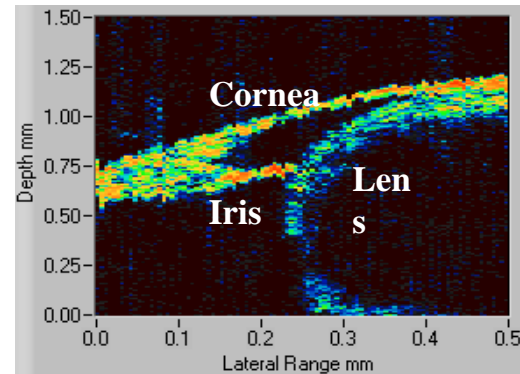
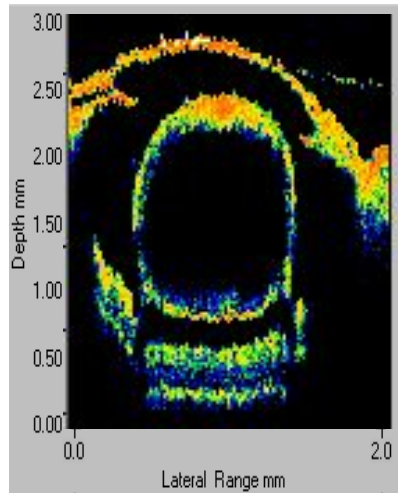
➤ Diagnosis

➤ Therapy

➤ Manipulation of single cells/sub-cellular objects

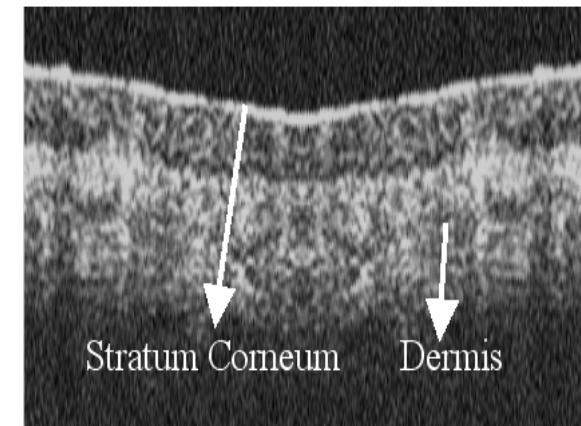
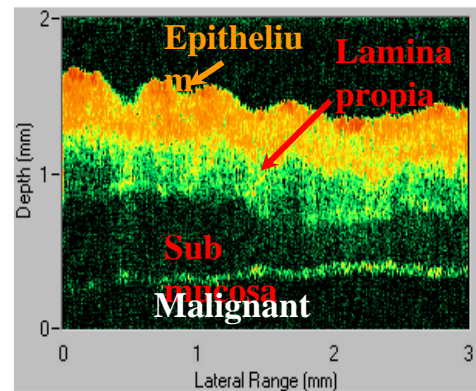
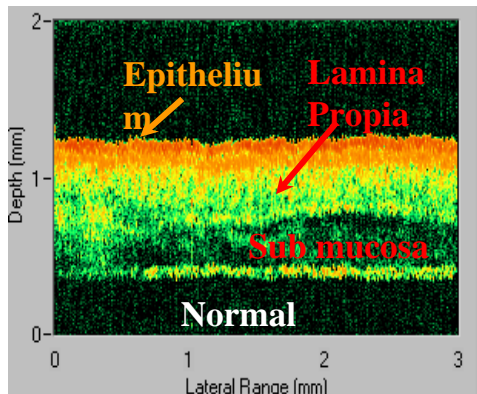
➤ Preparation of nanoparticles and exploration of their use for biomedical imaging, diagnosis and therapy

Imaging by Optical Coherence Tomography



OCT images of Zebra Fish Eye

Current Science, 90, 1506 (2006); Appl. Phys. B 87, 607 (2007)



**Real time hand held OCT set up
for dermatological applications**

**OCT images of (a) normal and (b) malignant
Hamster cheek pouch tissue**

OPTICAL SPECTROSCOPIC DIAGNOSIS OF CANCER

UNDERSTAND FLUORESCENCE FROM HUMAN TISSUE AND EVALUATE POTENTIAL OF USING IT FOR CANCER DIAGNOSIS

SIGNIFICANT VARIATION IN FLUOROPHORE CONCENTRATION IN N & M



System in use for the diagnosis of cancer of oral cavity

Diagnostic Algorithm	Predictive Accuracy for Validation Data Set	
	Sensitivity (%)	Specificity (%)
PCA	80	58
FLD	73	92
MRDF	95	96
SVM	93	95
RVM	93	95

Lasers Surg. Med., 33, 48 (2003)

J. Biomed. Opt., 10, 024034(2005)

Lasers Surg. Med., 36, 323 (2005)

Multi class Classification:

J Photochem. and Photobiol B, 85, 109 – 117 (2006)

PHOTODYNAMIC THERAPY

Chlorophyll derivatives (CP6, purpurin, ...)

Photochem. Photobiol. 75, 488, (2002),

Photophysical characterization

Photochem. Photobiol.Sci., 3, 231(2003)

Evaluation in cell lines and animal models

Photochem. Photobiol. Sci. 3,231-235 (2004);...

Use of CP6 for treatment of tumor in hamster cheek pouch

➤ Systemic delivery effective in small size tumors

Oral Oncology , 42, 77-82, (2006)

➤ Topical application more effective for large size tumors (8mm)

➤ Complete tumor necrosis and regression in small size tumor (<4 mm)

➤ Superficial necrosis and size reduction in large tumor, complete regression when PDT repeated 3-4 times at 72 hr interval

Photodynamic inactivation of antibiotic resistant bacterial cells

Current Microbiology 50, 277-280 (2005)

Toluidine Blue-Mediated Photodynamic Effects on Staphylococcal Biofilms

Antimicrobial agents and chemotherapy, (2008)

Application of Optical tweezers

BIOPHOTONICS

BIOPHOTONICS

Rotating Line Optical Tweezers Enables Controlled Intracellular Rotation of Microscopic Objects

Raktim Dasgupta, Samarendra Kumar Mohanty and Pradeep Kumar Gupta

Most of the techniques used for rotation of objects are limited to absorbing, birefringent or specially fabricated structures and hence are not suitable for rotation of biological objects.¹⁻³ Recently an interferometric approach suitable for rotation of a trapped biological object has been reported.⁴ However, this method has two important drawbacks: poor utilization of the trap laser power due to the loss in the generation of the required interference pattern and high susceptibility of the interference pattern to

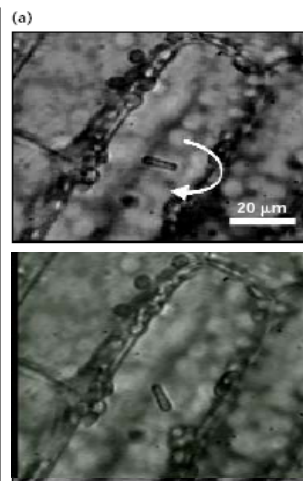


Figure 1. Rotation of an intracellular object using line optical tweezers. The rod shaped structure was trapped at 4 Hz. The direction of rotation is shown at 45° (b); 145° (c); and 235° (d). All the images were

Nanosecond Near-Infrared Laser-Assisted Microinjection Into Targeted Cells

Samarendra Kumar Mohanty, Mrinalini Sharma and Pradeep Kumar Gupta

Significance alteration in the context of a variety of applications in genetics, cell biology and biotechnology. Compared with conventional techniques, optoporation is more efficient, less tedious and offers the advantage of being usable on cells in suspension as well as on attached cells. Because the constituents of the cell membrane have strong absorption in the ultraviolet (UV) spectral range, lasers in this spectral range were the first to be investigated for optoporation. But the use of UV light raises concerns about damage to cells or even about exogenous biological material being transferred into the cell. Use of lasers of wavelength in the near-infrared region would be more

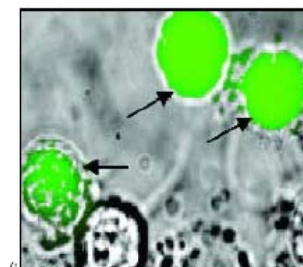
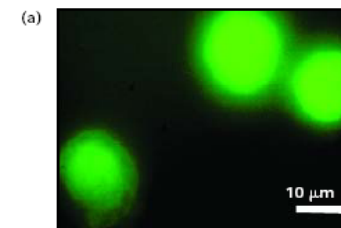


Figure 1. (a) Fluorescence image of cells expressing GFP. (b) Bright field and fluorescence images of cells.

Optics & Photonics News, Dec. 2003

Biophotonics

Self-Rotation of Red Blood Cells in Optical Tweezers: Prospects for High Throughput Malaria Diagnosis

Samarendra Kumar Mohanty, Abha Uppal and Pradeep Kumar Gupta

Infected red blood cells (iRBCs) are more rigid than the membrane of normal RBCs.¹ A measurement of membrane elasticity of a RBC can, therefore, be used for the detection of malaria. Interestingly, it has been determined that, in a hypotonic buffer medium (> 800 mOsm/kg osmolality), malaria-infected RBCs either do not rotate at all or rotate at a significantly slower speed because of their rigid membrane. A normal RBC, in contrast, rotates by itself when placed in a laser optical trap at the same trap-beam power. This difference in rotational speed has been exploited for the detection of malaria-infected cells.²

In a hypotonic buffer, a monocyte-shaped normal RBC rotates when it is optically trapped with trap-beam power beyond 40 mW (Fig. 1) because of the torque that is generated on the cell by the transfer of linear momentum from the

OPTICS IN 2004

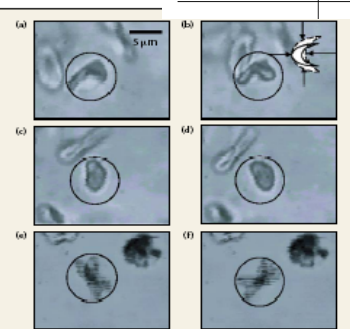


Figure 1. Rotation of a normal RBC trapped by optical tweezers. The cell (circled) was suspended in a hypotonic buffer and trapped at power levels that varied from (a) 40 mW to (b) 200 mW. Figure 1(c) and (d) show a schematic of the deformation observed in the horizontal cross section of a RBC structure at a higher trap-beam power (solid circle). The dotted circle corresponds to the shape observed without the trapping beam. Arrows illustrate the transverse gradient force of optical tweezers. Figure 1 (c) and (d) show time-lapsed digital video images of RBC rotation at a buffer conductivity of 1,000 mOsm/kg. Images in (c) and (d) represent an conductivity of 1,250 mOsm/kg. The trap power was 40 mW and the time lapse between consecutive frames was 80 ms. From the sequence of digitized frames, the speed of rotation was estimated to be 24 rpm at 1,000 mOsm/kg and 200 rpm at 1,250 mOsm/kg.

Optics & Photonics News, Dec. 2004

Transport of Microscopic Objects Using Line Optical Tweezers: Manipulation of Neuronal Growth Cones

Samarendra Kumar Mohanty, Mrinalini Sharma, Mitradas Panicker and Pradeep Kumar Gupta

The transport of microscopic objects plays an important role in several biological processes that are crucial for cell functioning. By becoming able to effect controlled transport of intracellular objects, researchers can not only understand these fundamental processes better but also manipulate the functionality of living cells.

We have shown that line optical tweezers, with an asymmetric intensity distribution along the major axis of the

elliptical trap beam, can be used for efficient and controlled transport of microscopic objects in a plane transverse to the direction of beam propagation.¹ The asymmetry in the intensity distribution of the trap beam about its center results in a potential well that is asymmetric about the center of the beam.

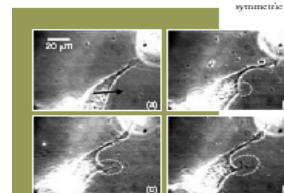
Thus, particles at the steep end of the potential well are pulled toward the potential minima, accelerate, and are ejected in the direction toward the lower intensity. Since the gradient force is large and asymmetric in the other two orthogonal directions, the particles are constrained to move along the major axis of the line tweezers.

We controlled the depth and the asymmetry of the potential well by a control on trap-beam power and by a change in the angle of incidence of the laser beam with respect to the optic axis of the microscope objective. To change the direction of transport, we rotated the cylindrical

gradient end of the elliptical focus such that the tip of the growing edge was closer to the lower gradient force. Since the neuronal growth is believed to involve transport of axons in the direction of the growth cone,² the observed enhancement in growth can be attributed to diffusion of axons.

Compared to a growth rate of $1 \pm 1 \mu\text{m/h}$ observed for untrapped neurons, the lamellipodia extension rate in a neuron subjected to line tweezers was estimated to be $32 \pm 6 \mu\text{m/h}$. The asymmetric transverse gradient force could also be used for induction of new growth cones from the neuronal cell body (see figure). The optically induced growth cones showed branching similar to that observed in the natural process of growth.

However, the growth rate of these induced cones was lower ($15 \pm 5 \mu\text{m/h}$) than that achieved for natural growth cones. This approach could be used to change the orientation of a growth cone to bring it into close proximity with a cone of another neuron. The ability to exert such control on neuronal growth cones may prove useful for establishing a connection between two neurons. *doi:10.1002/olp.10004*



Optics & Photonics News, Dec. 2005

Interaction of organically modified silica nanoparticles with molecules of biomedical relevance

Silica Nanoparticles

Biocompatible & nontoxic

Hydrophilic in nature

(reduces the problems of non-specific binding and clustering)

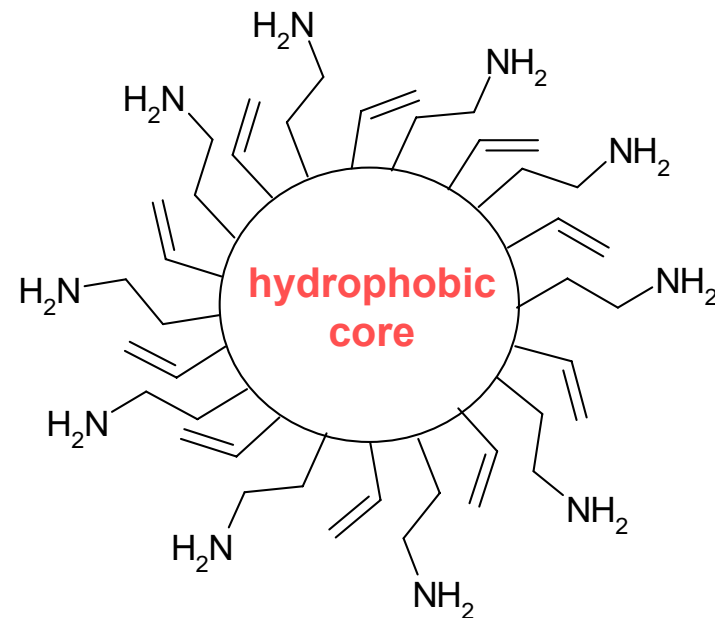
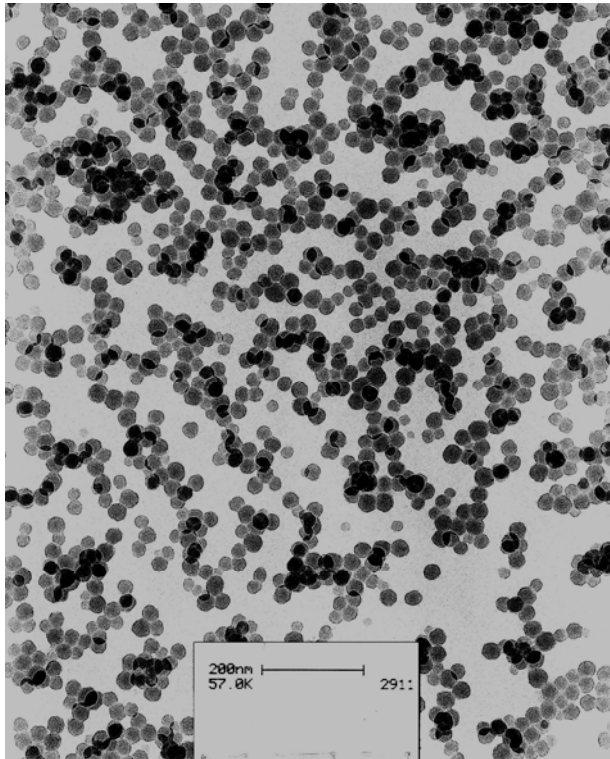
Chemical inertness & transparency

Less prone to attack from microbes.

Easy to prepare, modify surface and separate via centrifugation

Imaging & Drug delivery

Organically modified SiNPs (~25 nm) were prepared using Vinyl triethoxysilane (VTES) and 3-aminopropyl-triethoxysilane (APTS) using a micellar template

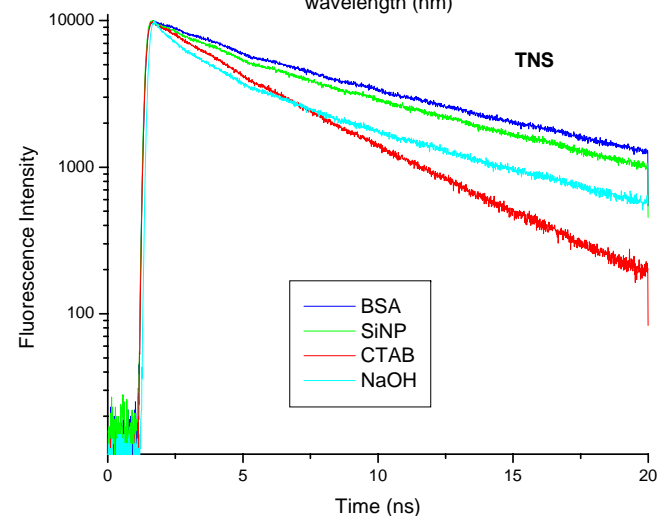
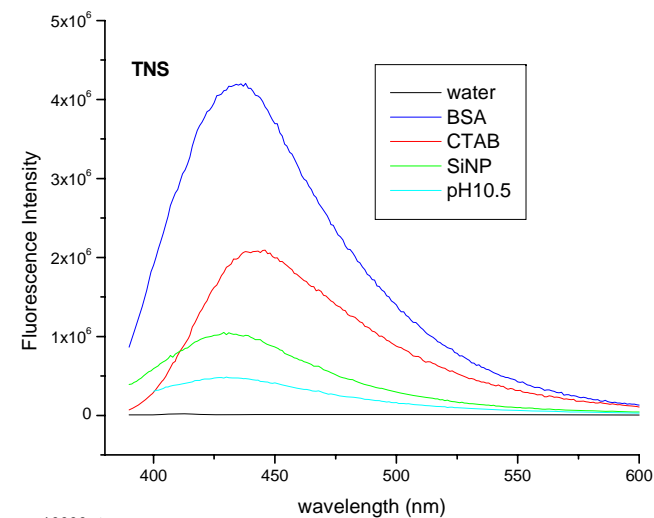
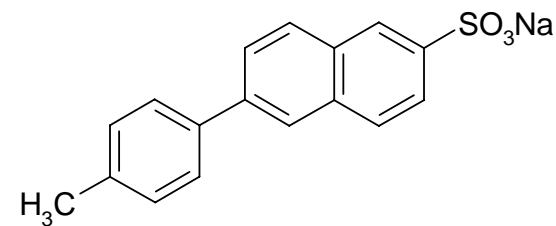
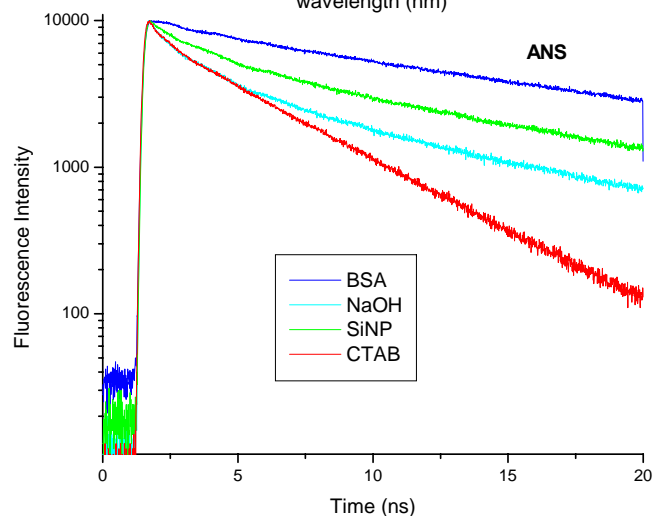
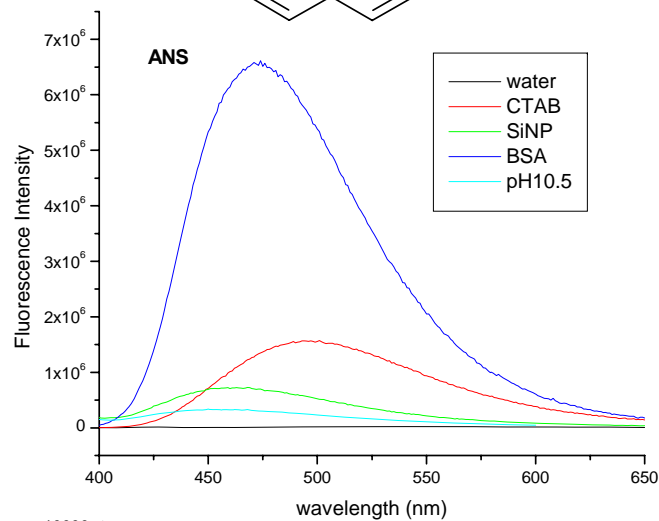
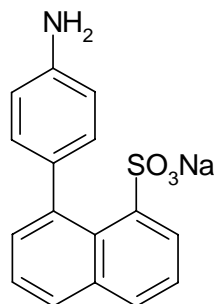


At neutral water the amine groups present at the surface are expected to be positively charged as the pK_a value of the 3-aminopropyl group of APTS is ~ 9

ANS

Polarity sensitive fluorescence probes

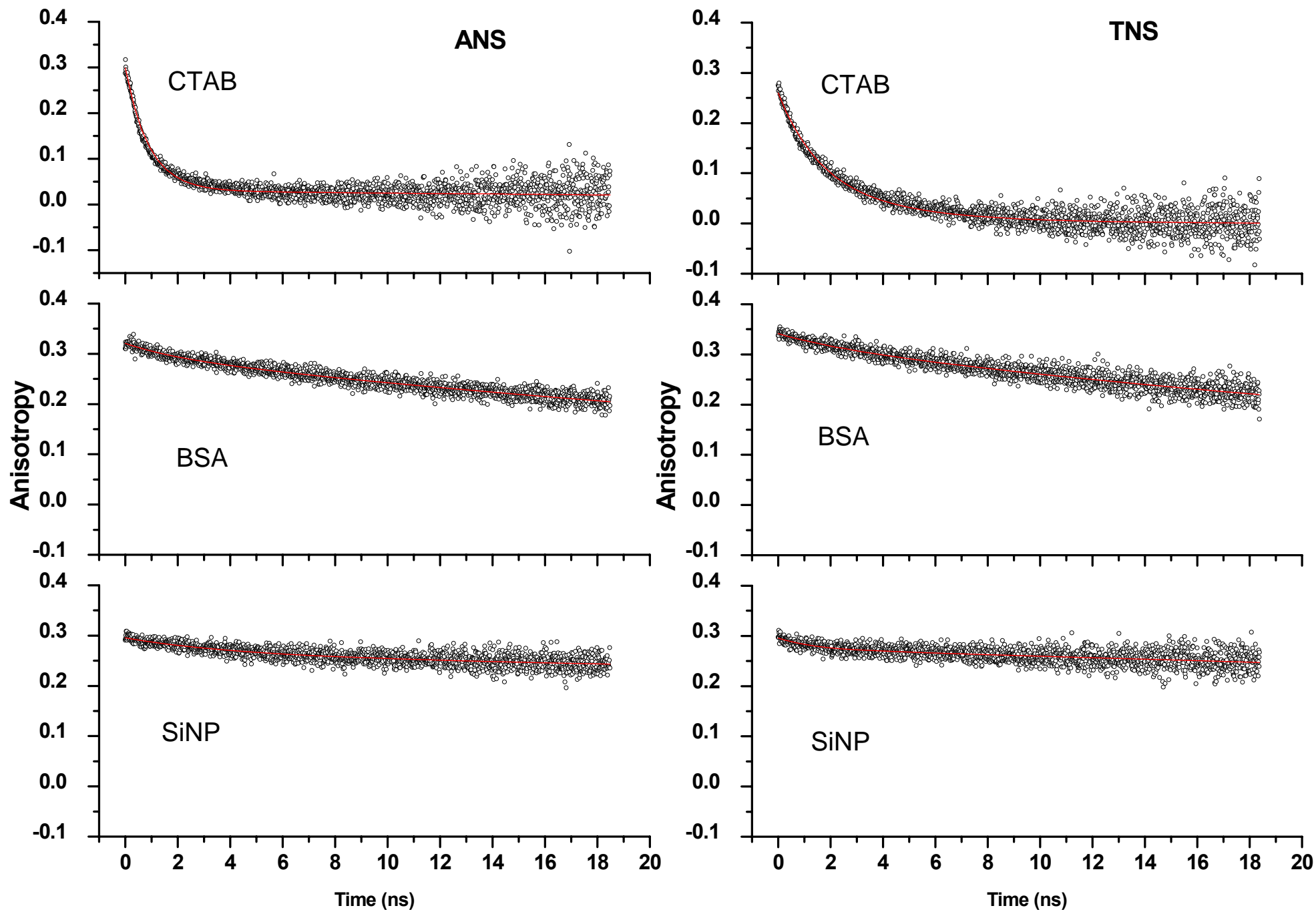
TNS



Water
CTAB (micelle)
SiNP (neutral)
SiNP (basic)
BSA (protein)

Steady state & time resolved fluorescence

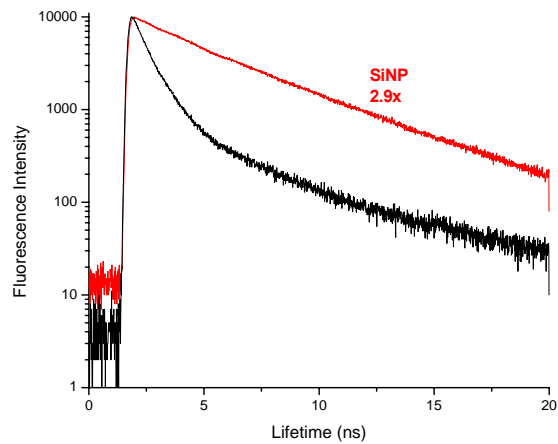
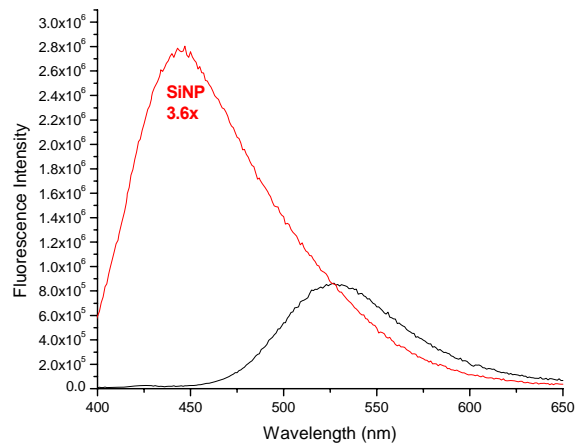
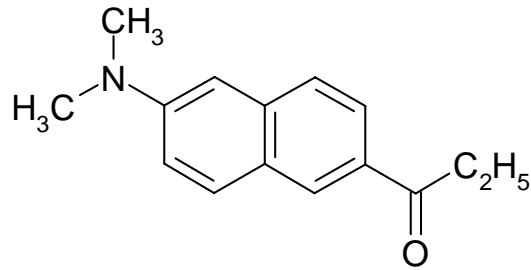
Time resolved polarized fluorescence



- **A comparison of the photophysical parameters of ANS & TNS in SiNP, protein and micellar environment suggests the presence of fluorescence quenching in SiNP, which might be static in nature.**
- **Both ANS and TNS reside at the interface of CTAB micelles. With SiNP, ANS & TNS resides at interface (electrostatic interaction) and in the core (hydrophobic interaction).**
- **Fluorescence polarization measurements suggests that they are tightly bound to SiNP and protein compared to CTAB micelles.**

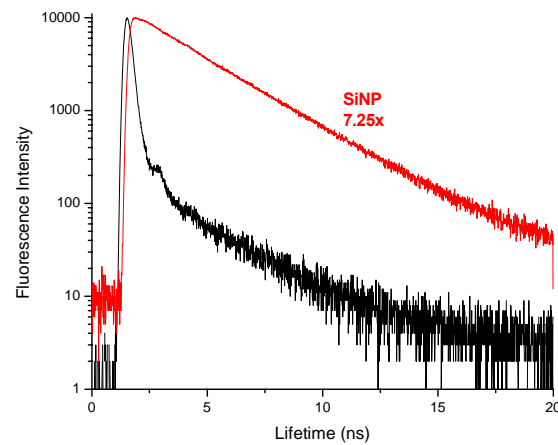
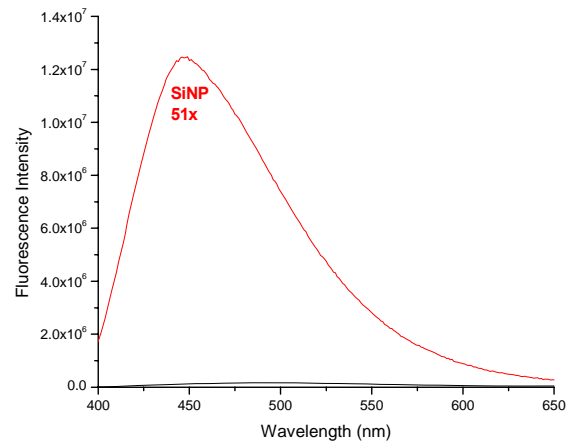
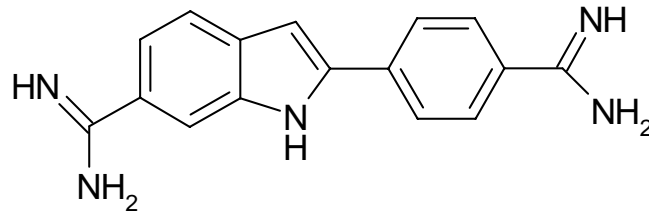
polarity

PRODAN



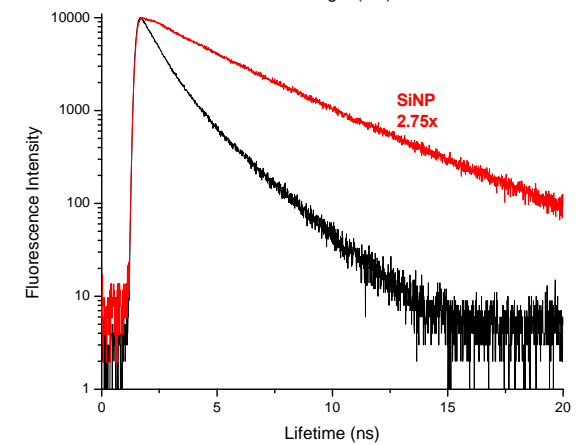
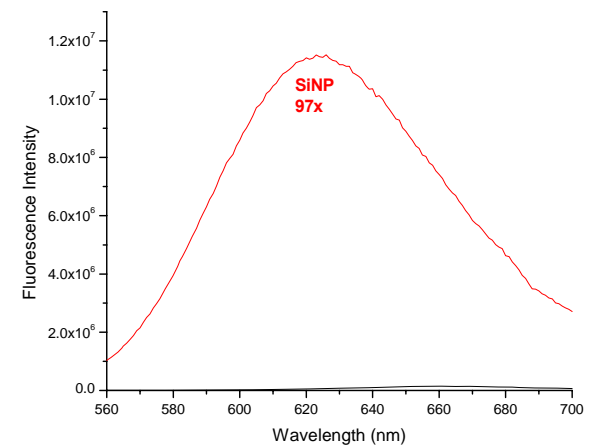
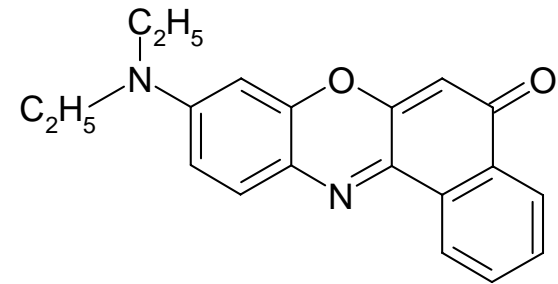
nucleic acid stain

DAPI

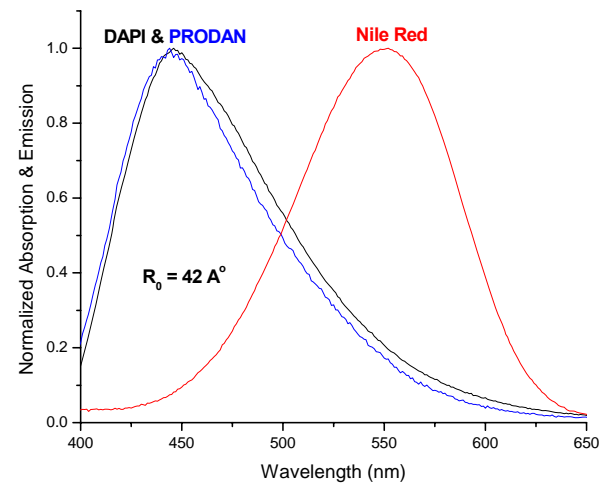


hydrophobic

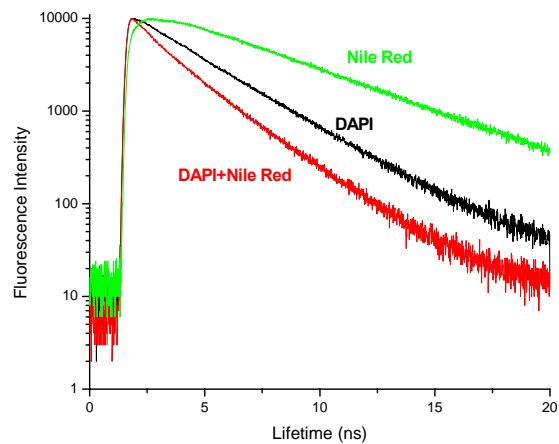
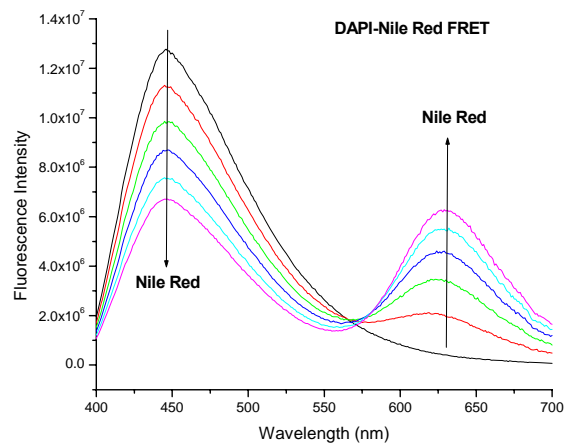
Nile Red



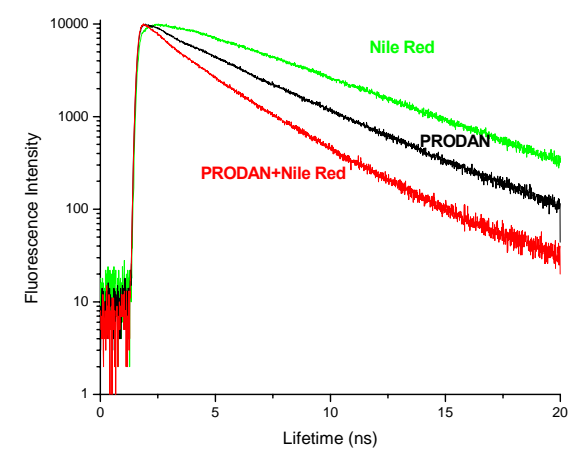
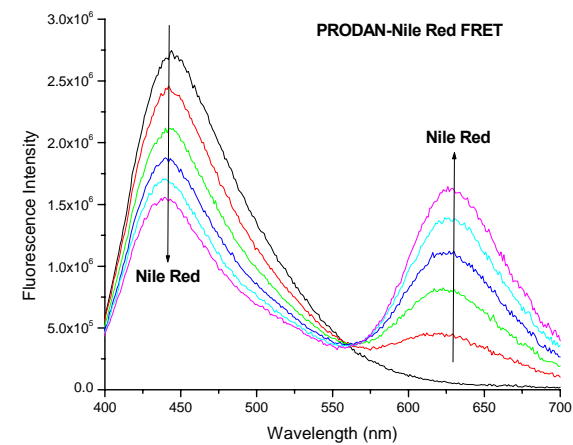
Forster Energy transfer in SiNP



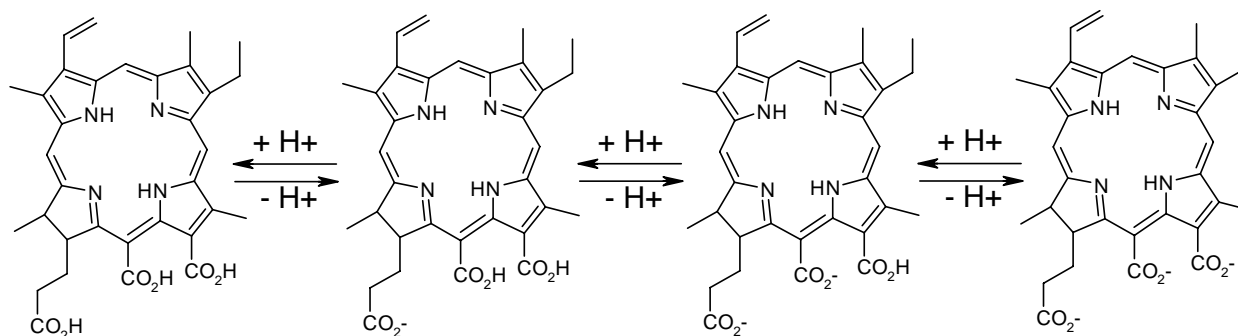
DAPI-Nile Red



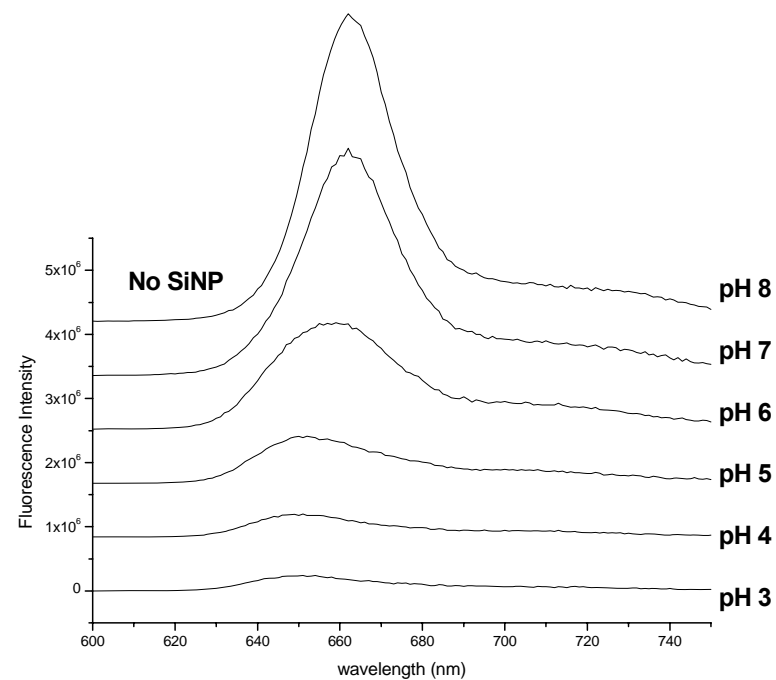
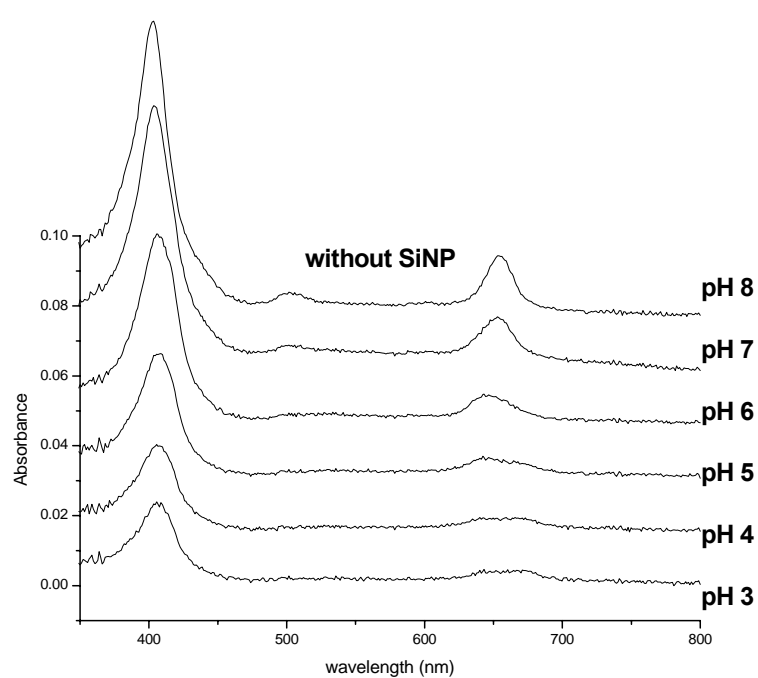
PRODAN-Nile Red



Chlorin-p6

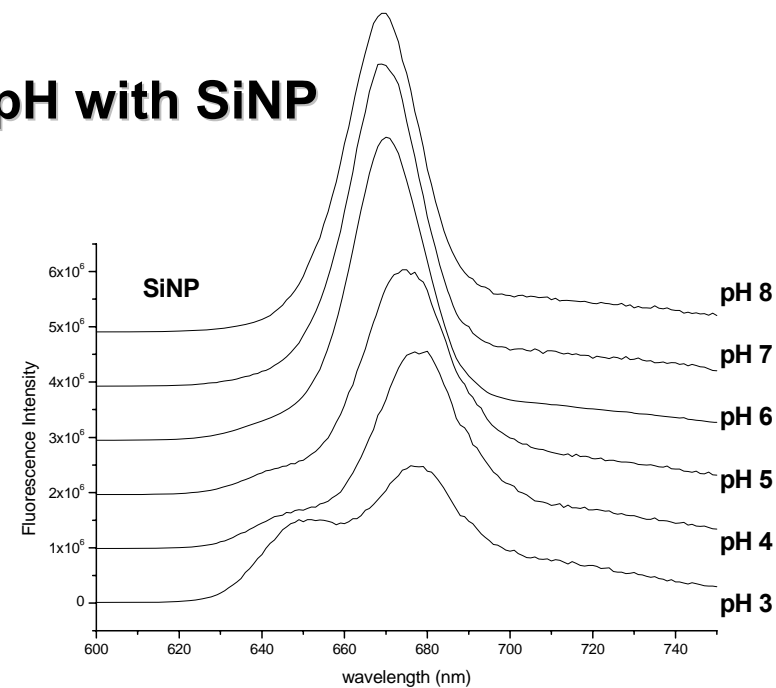
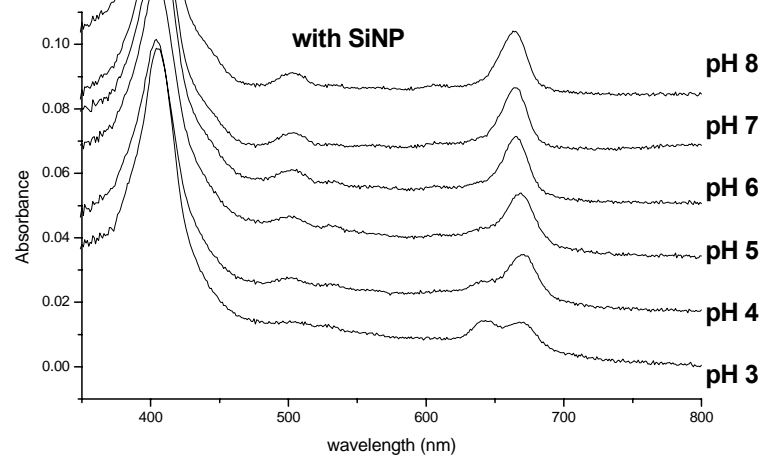


Non-fluorescent aggregates formed at low pH due to successive protonation of the COOH groups

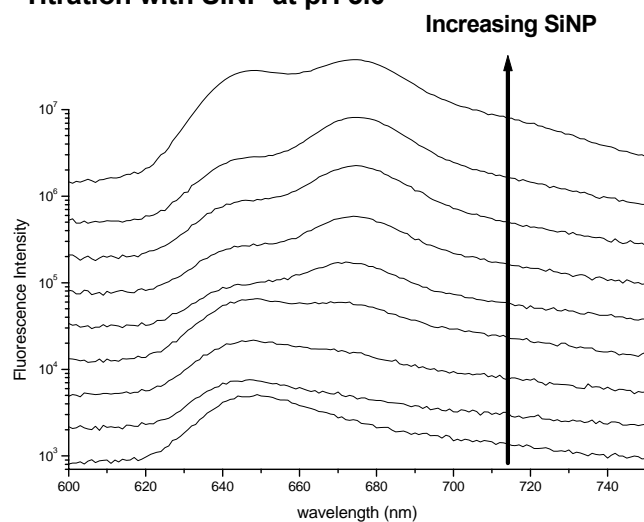


Absorption & emission at different pH

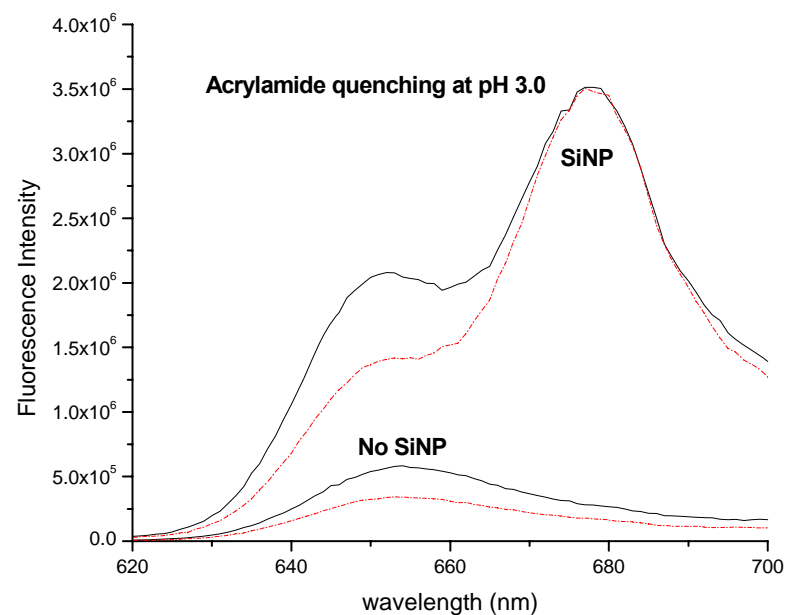
Absorption & emission at different pH with SiNP



Titration with SiNP at pH 3.0



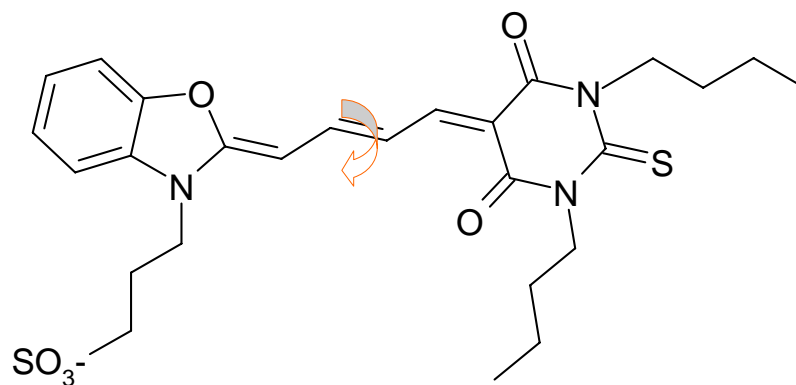
Emission titration with SiNP at pH 3.0



Effect of a quencher

- **Acid-base ionization equilibrium is significantly affected as a result of strong electrostatic binding between the negatively charged drug and SiNP.**
- **The spectroscopic signature of the drug bound to SiNP suggests that the tri-anionic form of the drug remains bound to the positively charged SiNP at pH 8.0.**
- **At pH 5.0 and 3.0 the formation of hydrophobic aggregates is disrupted significantly due to the presence of electrostatic binding force, which competes with intermolecular hydrophobic forces.**
- **The interplay of hydrophobic and electrostatic forces in the drug-nanoparticle binding process might affect the relative uptake and photodynamic efficacy of the free drug and the drug-nanoparticle complex in cancer cells.**

Merocyanine 540



Anionic photosensitizer

Aggregation & photoisomerization

Weakly fluorescent

Photodegradable

Low singlet oxygen quantum yield

In water

Reduce photoisomerization



Enhance $^1\text{O}_2$ yield & photostability?

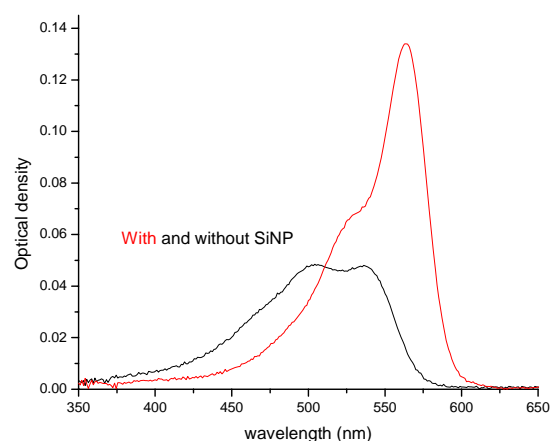
**Binding with liposomes reduces photoisomerization rate
and increases $^1\text{O}_2$ yield by ~20 times**

M. Krieg, *Biochim. Biophys. Acta*, 1105, 333 (1992)

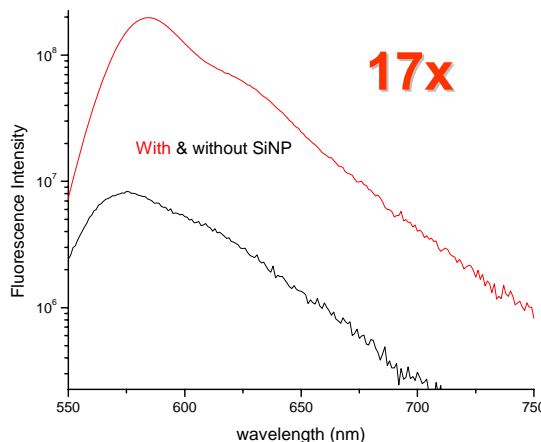
**Use positively charged silica nanoparticles (SiNP)
to reduce photoisomerization rate??**

Interaction between MC540 and SiNPs in aqueous media

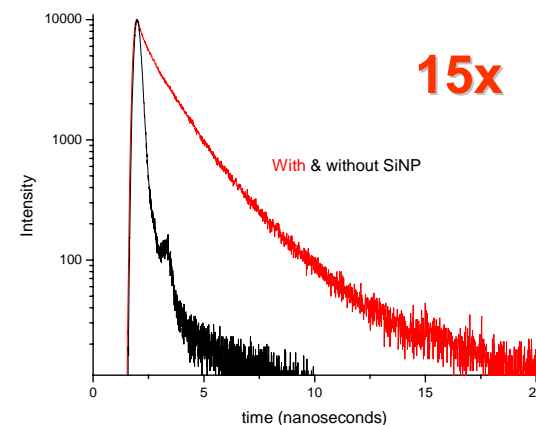
Spectroscopic investigation



Absorption



**Fluorescence
steady state**



**Fluorescence
time resolved**

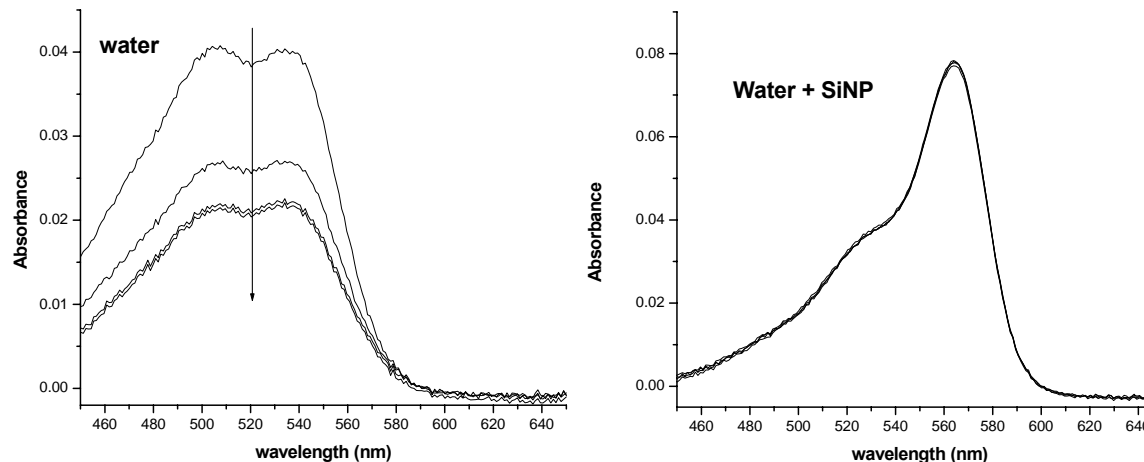
Enhanced **absorption** and **fluorescence** in presence of **positively charged SiNPs**

Fluorescence parameters in different environments

Environment	Absorption	Fluorescence (quantum yield)	Fluorescence lifetime (ns)	Radiative rate ($\times 10^{-9}$)	Nonradiative rate ($\times 10^{-9}$)
Water	505/536	570 (0.03)	0.10	0.31	9.70
Liposome	565	583 (0.49)	1.5	0.33	0.34
Water+ SiNP	563	583 (0.53)	1.5	0.36	0.32

Decrease in nonradiative rate \longrightarrow Increased photostability?

Photobleaching of free dye and dye-SiNP complex



Photostability **increases** in presence of SiNPs

Cellular uptake & phototoxicity

Target MCF cells

Plated cells in 60 mm petri dish
Incubated in serum free minimum essential media for one hour
(MC540 1 μ M & SiNP 10-20 μ gm/mL)

Cellular uptake

Fluorescence microscopy of
free drug & drug-SiNP complex
(Ex = 530 / Em > 590)

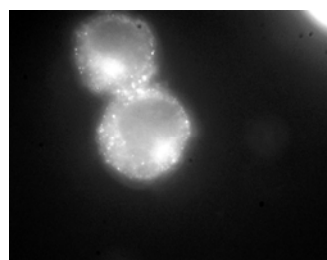
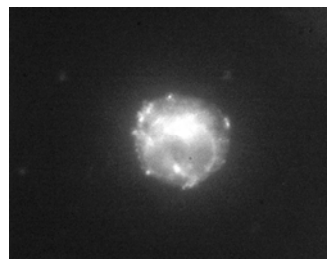
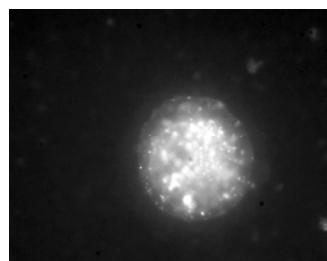
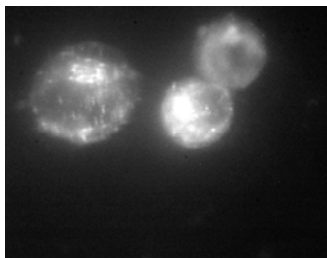
Light induced toxicity

Irradiated at 450-650 nm
Light dose: 1.8, 3.6 and 5.4 kJ/m²)

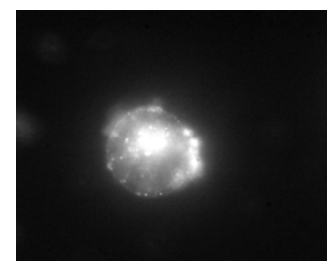
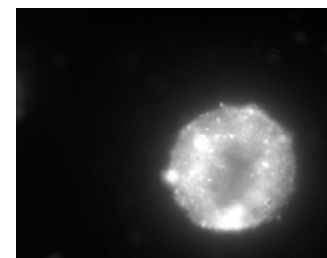
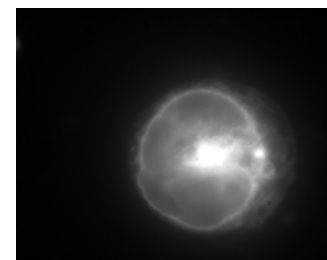
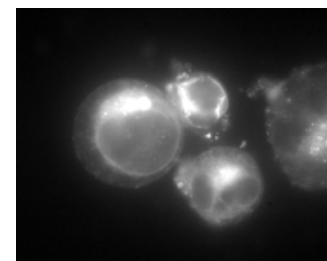
- Only MCF cells **control**
- MCF cells + drug
- MCF cells + SiNP
- MCF cells + SiNP-drug complex

Monitoring cell survival **after 24 hours**
using MTT assay

Cellular uptake : Fluorescence microscopy



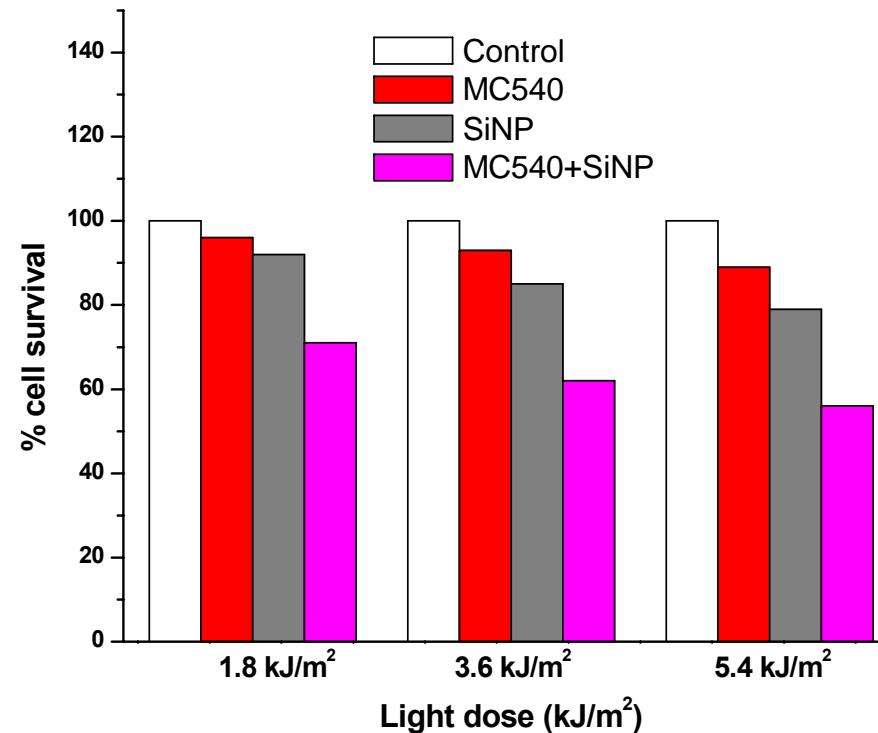
1 μ M MC540



1 μ M MC540 + 20 μ gm/mL SiNP

Light induced toxicity

(No dark toxicity observed)



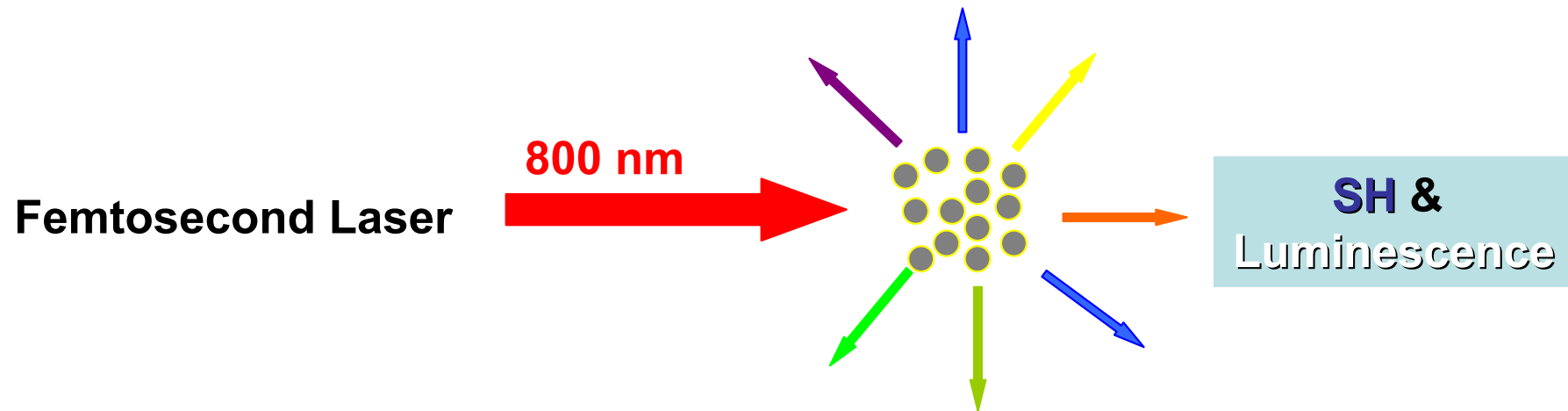
Drug = 1 μ M
SiNP = 20 μ gm/mL

The light dose dependent cell killing were observed to be the **highest** for the drug-SiNP complex

Summary

- The **electrostatic binding** between **Merocyanine 540** and **SiNPs** has been characterized using absorption and fluorescence spectroscopy
- The **binding** resulted in significant changes in the absorption spectra. The fluorescence intensity and lifetime gets **enhanced by more than an order of magnitude**
- The results obtained suggest that **this is due to the reduced photoisomerization rate** of the dye bound to the nanoparticle
- Consistent with the expectation that a reduction in the photoisomerization rate should **enhance the singlet oxygen yield** of the dye, the **light induced toxicity** of the **dye-nanoparticle complex** (tested with MCF cells) was observed to be **higher** compared to the **free dye**

Multiphoton-absorption induced processes in silver nanoparticles under femtosecond laser excitation



SH generation

$$I_{2\omega} = G < N_s \beta_s^2 + N_a \beta_a^2 > I_{\omega}^2 e^{(-N_a(2\alpha_{\omega} + \alpha_{2\omega})l)}$$

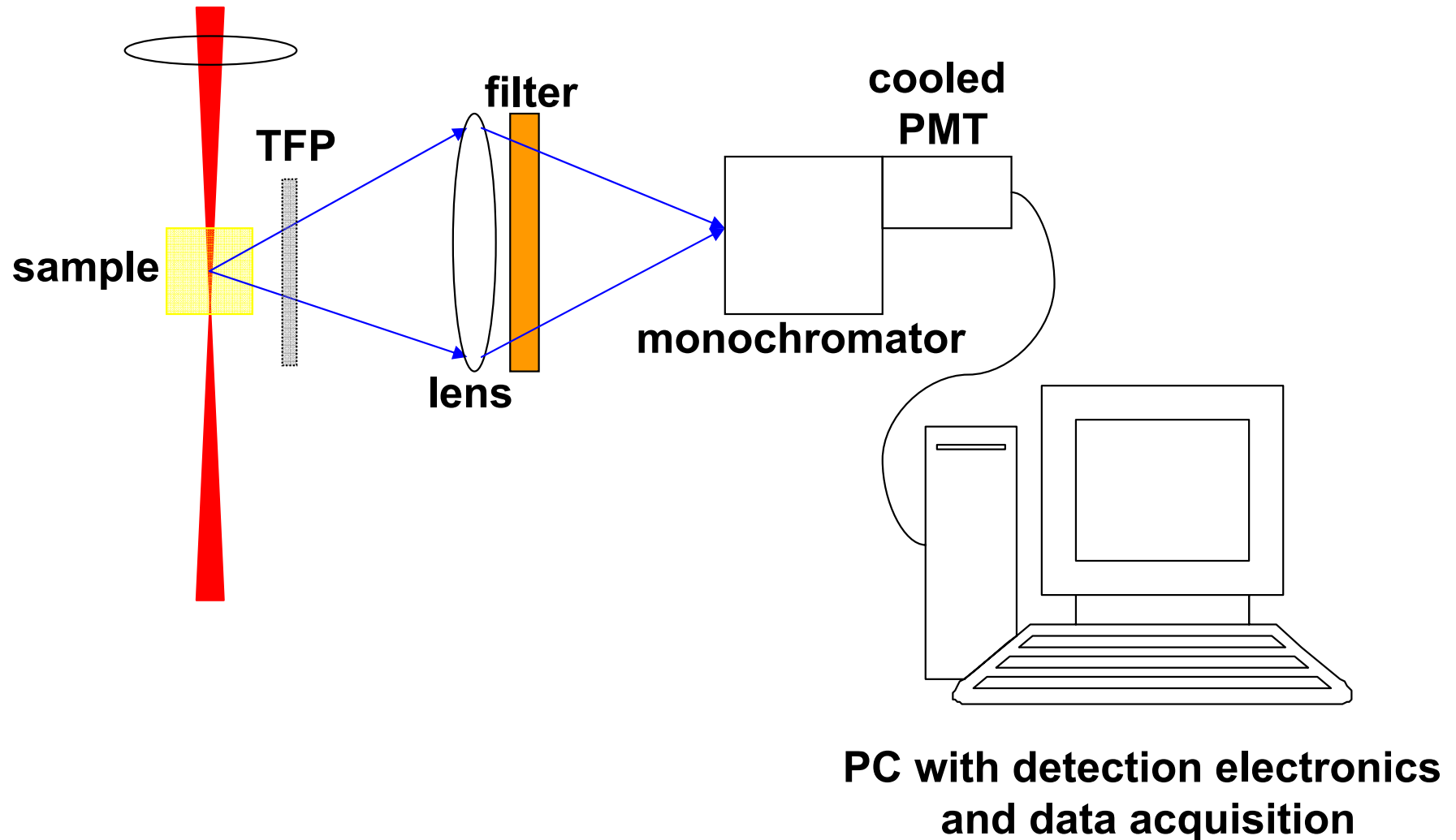
Luminescence

Radiative **electron hole recombination** in the **interband transitions** between the **sp** and **d** bands

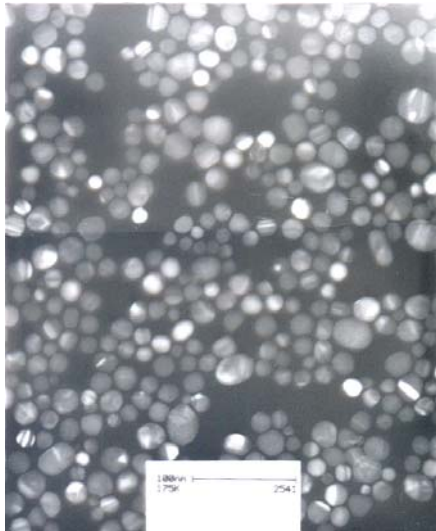
*Both depends critically on the shape
and size of the nanostructures*

Experimental Setup

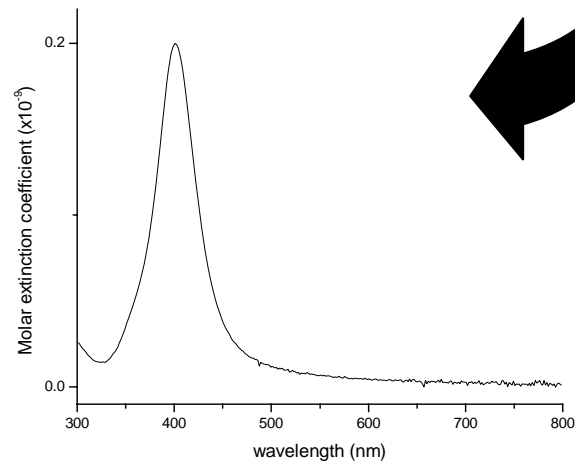
**~100fs Ti-Sapphire laser
780 to 920 nm
vertically polarized**



SH from Silver Nanoparticles

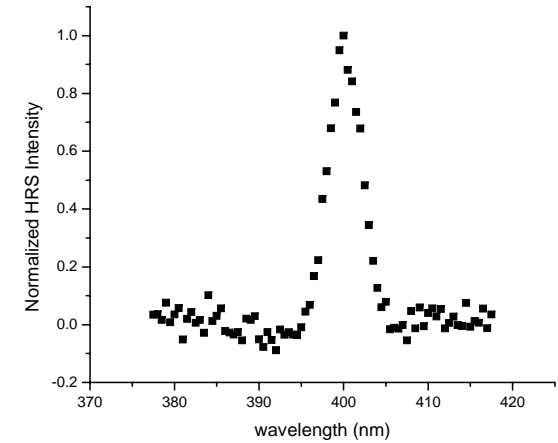


TEM
picture

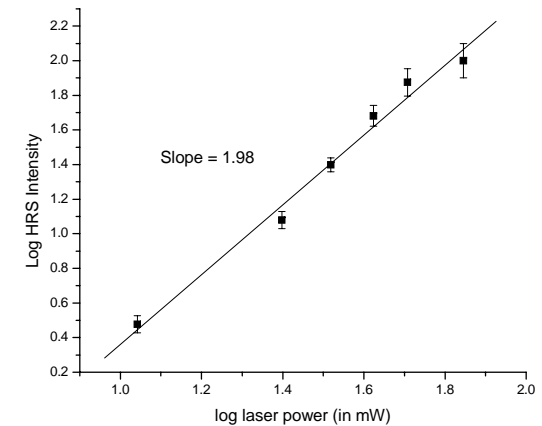


Typical extinction spectra

SH
spectrum



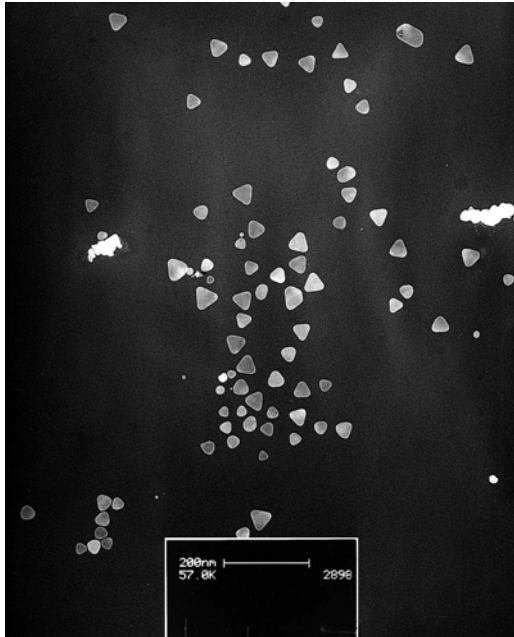
SH intensity
vs. incident
laser power



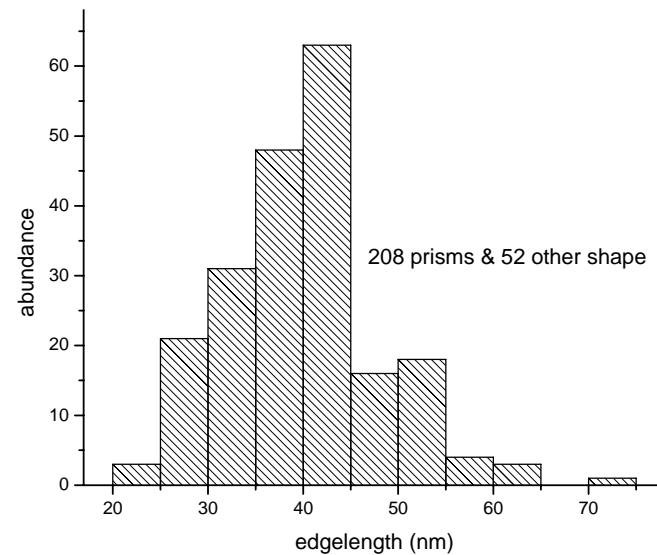
Excitation source:
Femtosecond laser @ 800 nm

Silver Nanoprisms

Preparation: Chemical method (Adv. Materials, 17, 2005, 412)



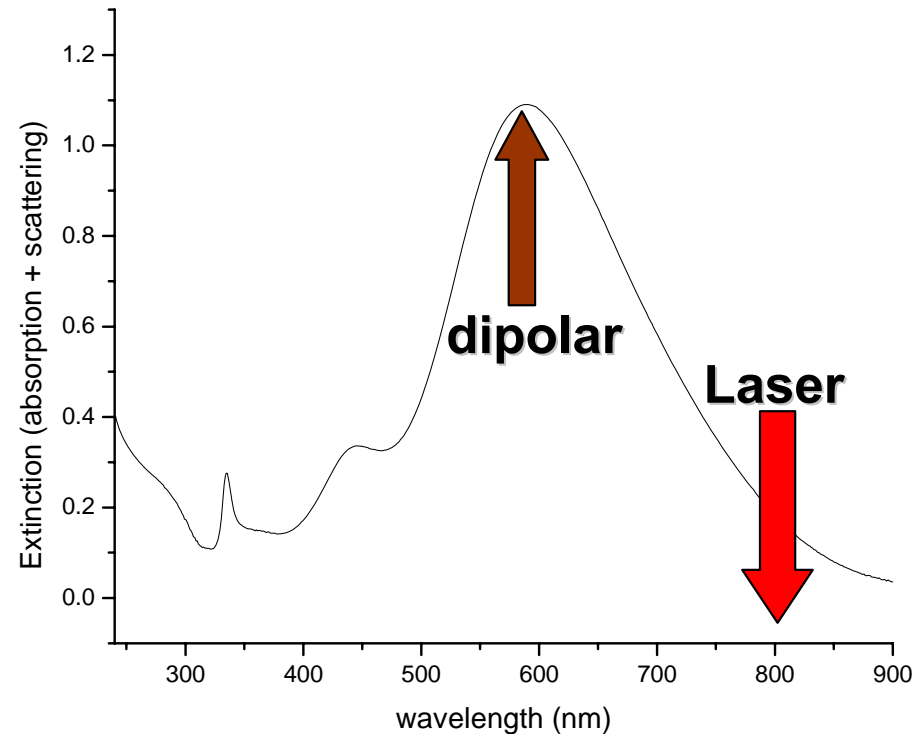
**Typical TEM image of
Silver nanoprisms**



**Histogram of the edge
length distribution**

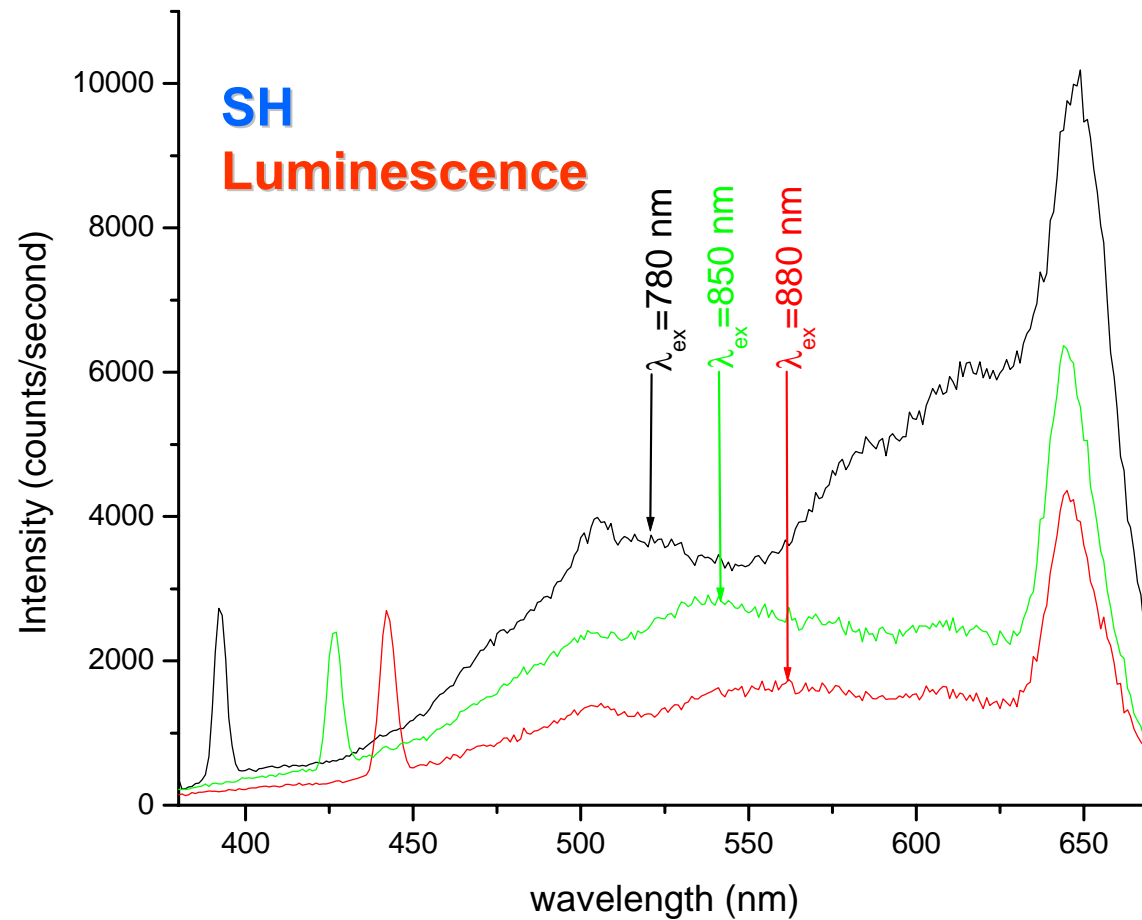
Average edge length: 35-45 nm
Average thickness: 4-5 nm

Typical extinction spectrum



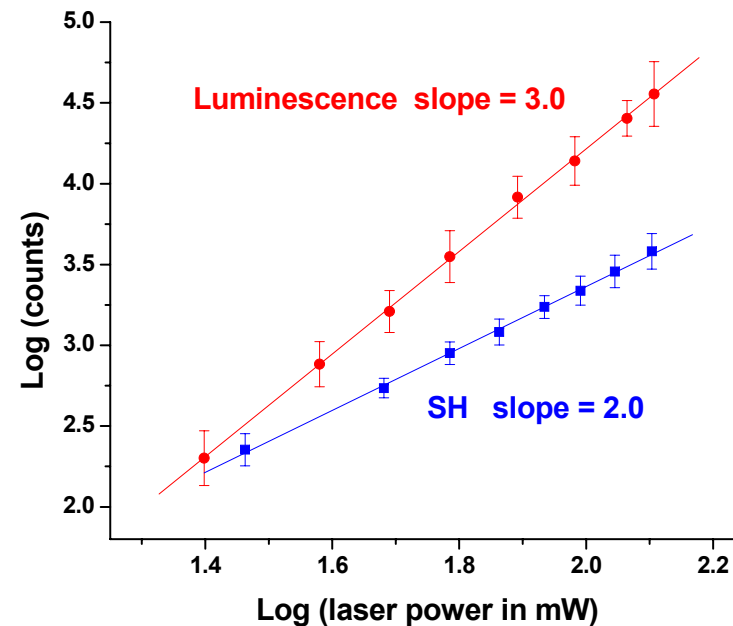
- **Dipolar SPR band** is very sensitive to the environment
- Attractive candidate for various **sensing applications**
- Many of the sensing applications are based on **ensemble average spectroscopic properties**
- Important to study the **ensemble spectroscopic properties** of the nanoparticles alone

Multiphoton absorption induced processes in Ag nanoprisms



- Luminescence intensity **excitation wavelength dependent**
- The onset of luminescence precedes the **SH** peak
(> **second order process??**)

Power dependence of SH and luminescence

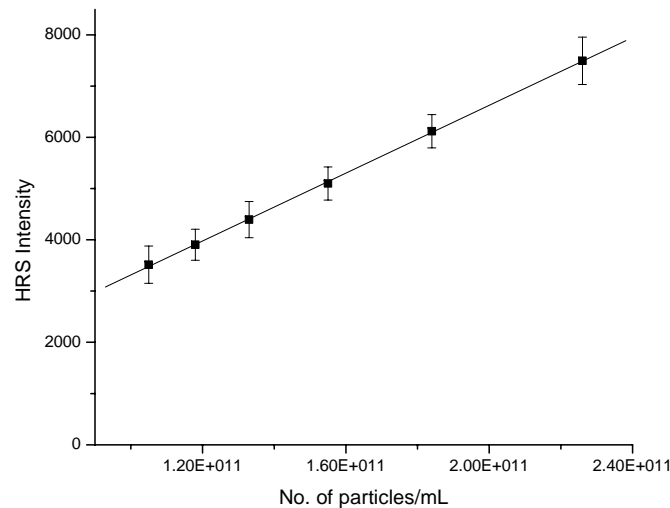


Luminescence from the **silver nanoprisms** is a **three-photon induced process**

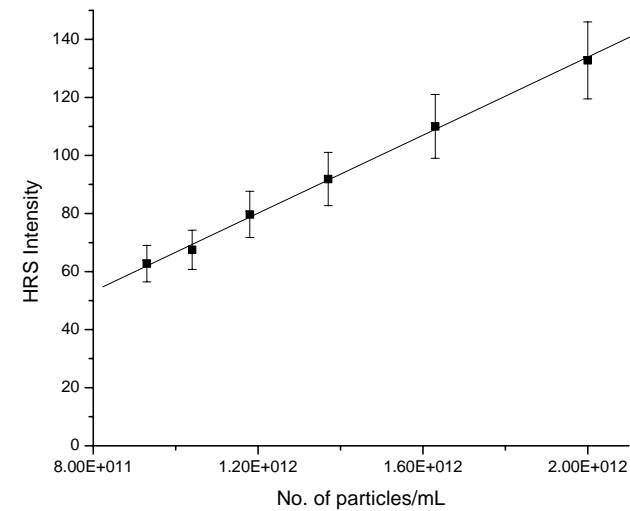
- Coupling of incoming (excitation) and outgoing (luminescence) with localized surface plasmons
- Presence of sharp corners/tips where SP field is intense

Hyperpolarizability (β) measurement of spheres & prisms

$$I_{2\omega} = G \langle N_s \beta_s^2 + N_a \beta_a^2 \rangle I_{\omega}^2 e^{(-N_a (2\alpha_{\omega} + \alpha_{2\omega}) l)}$$



Prisms



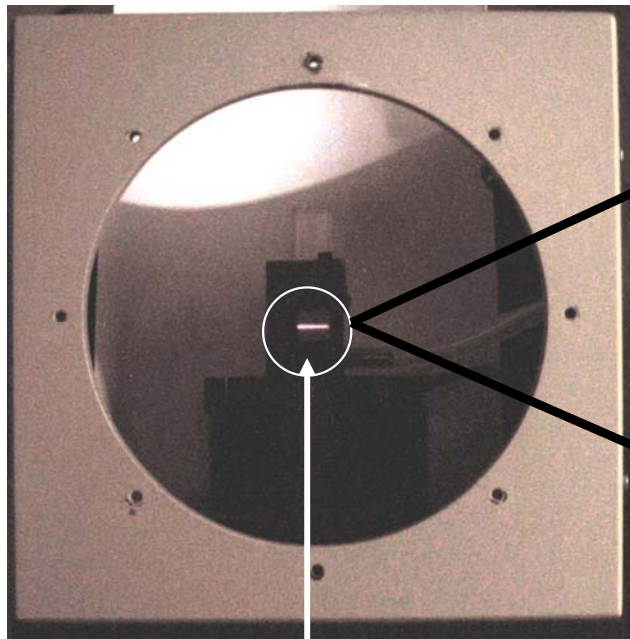
Spheres

For 850 nm excitation the β' value for nanoprisms and spheres are $35000 \pm 5000 \times 10^{-30}$ esu and $2000 \pm 800 \times 10^{-30}$ esu respectively

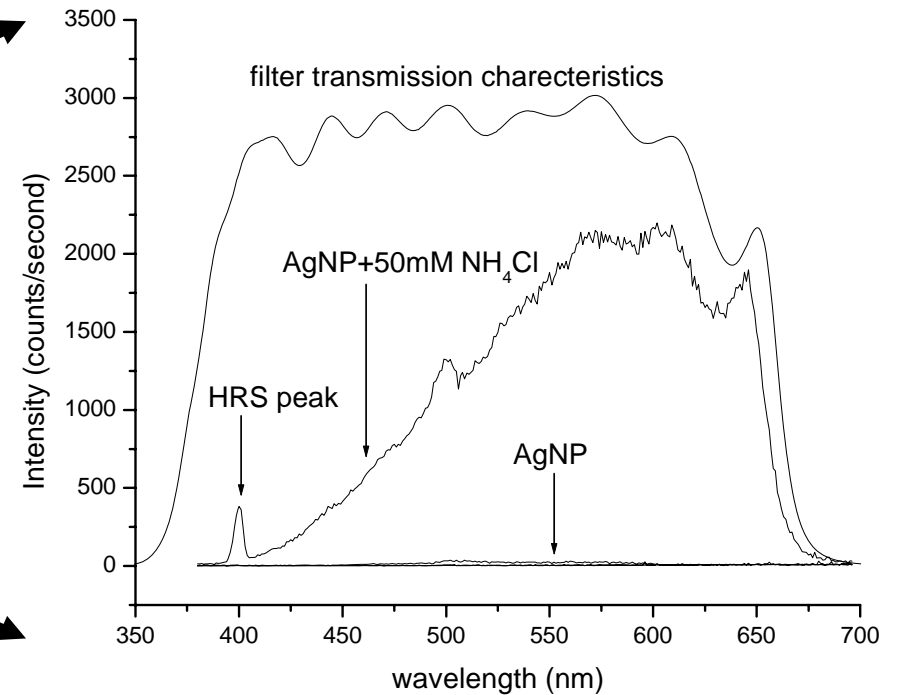
Effect of addition of electrolytes on nanospheres

- Addition of salt reduces the thickness of Electrical Double Layer
 - Reduces electrostatic repulsion
 - Formation of aggregates
- Tremendous increase in β : enhanced SH (and SERS)

Salt effect on Ag Nanospheres

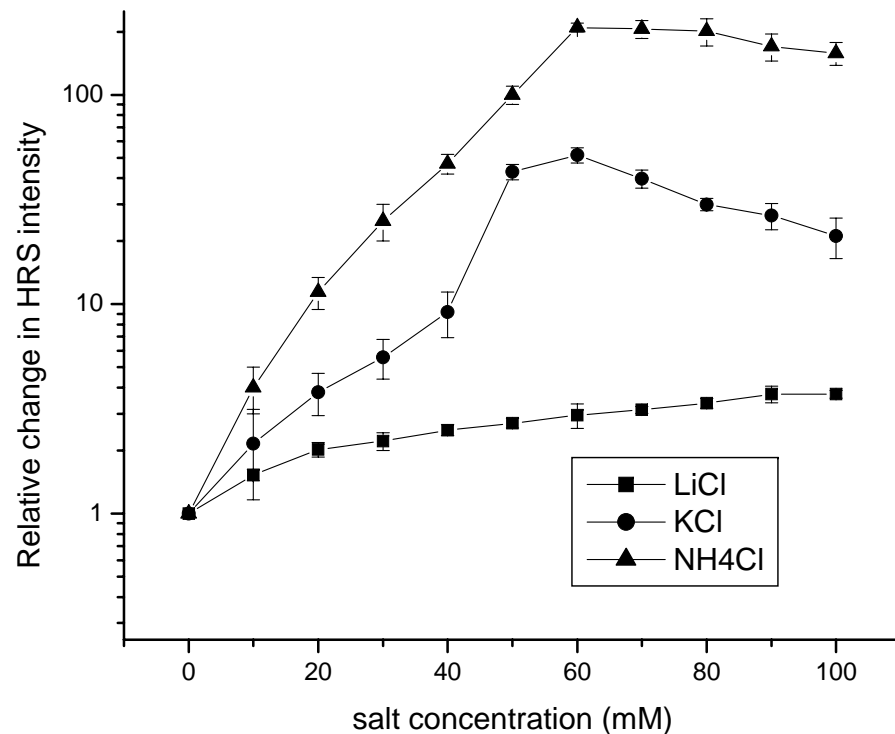


Ag Nanoparticles with
50 mM NH_4Cl



SH & luminescence
from aggregated AgNPs

Relative **SH** enhancement: Salt effect



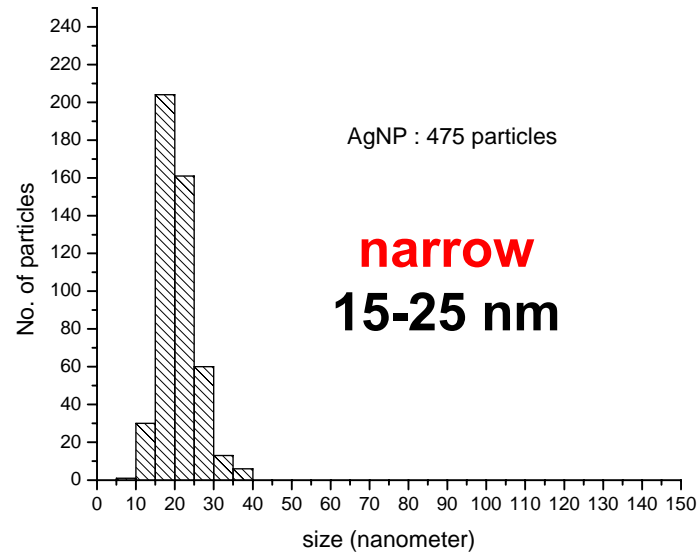
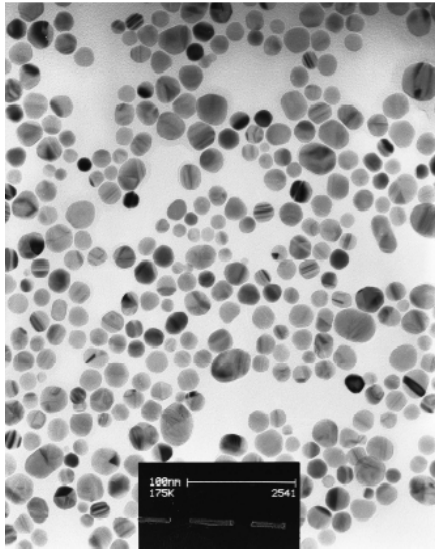
LiCl : ~4 times
KCl : ~50 times
NH₄Cl : ~200 times

$r_{\text{Lithium}} < r_{\text{Pottasium}} < r_{\text{Ammonium}}$
0.68 Å⁰ 1.33 Å⁰ 1.61 Å⁰

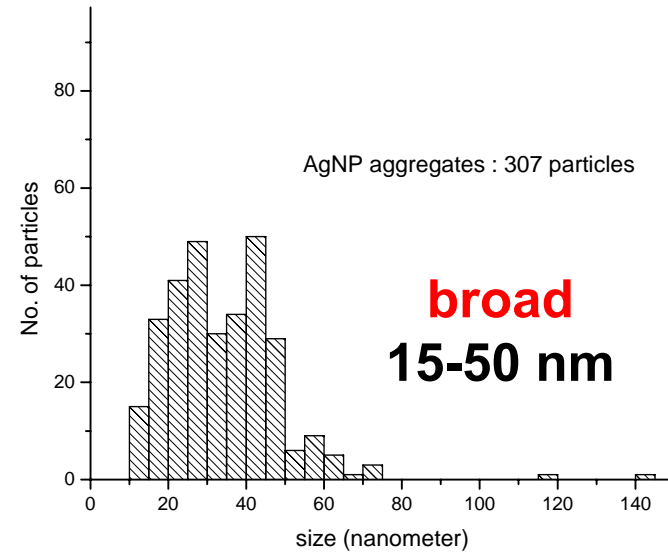
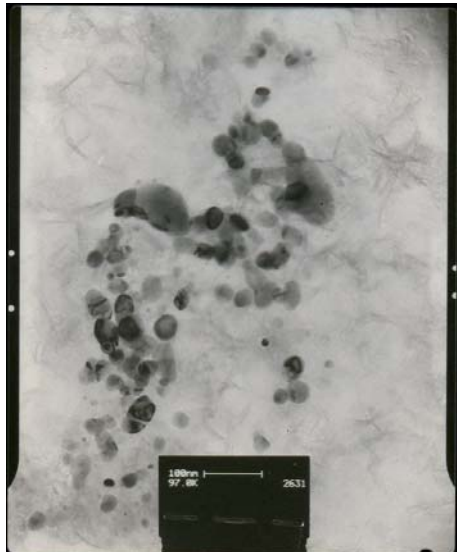
Size and hence the **charge density** of the cation plays an important role in colloidal **aggregation**

Particle size distribution

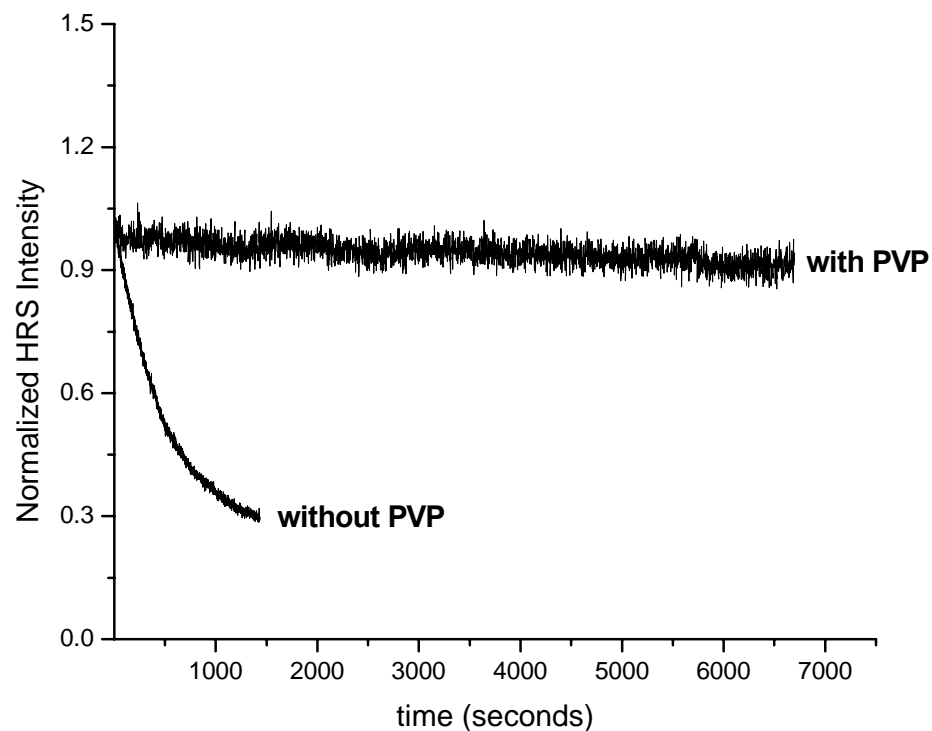
w/o electrolyte



with electrolyte

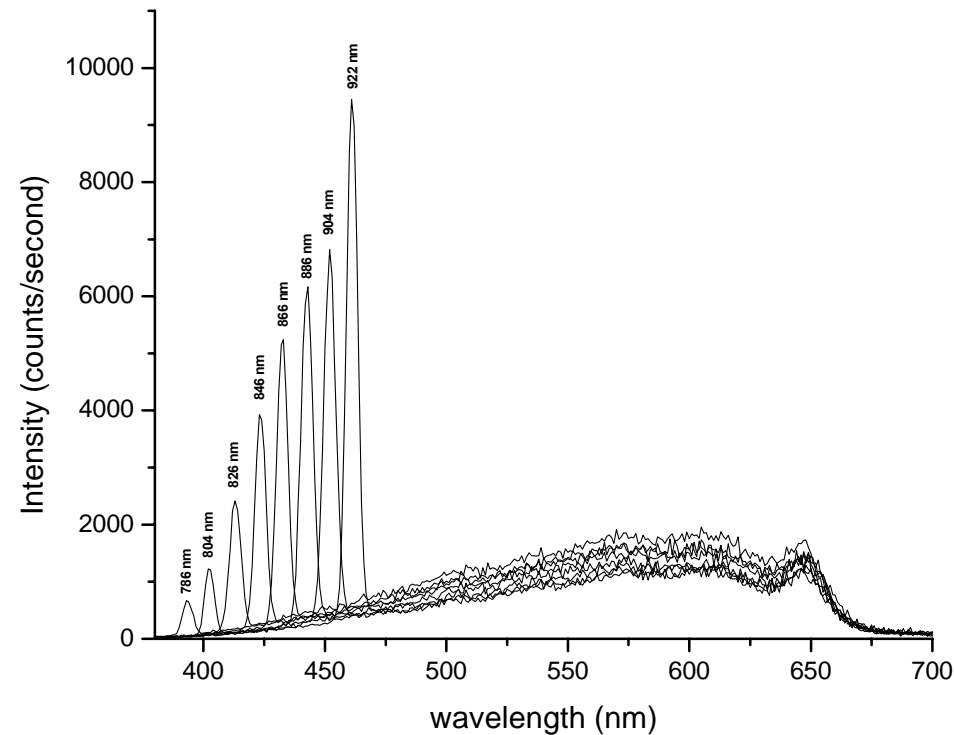


Time dependent change of **SH** intensity of NH_4Cl induced aggregates : Effect of addition of a polymer



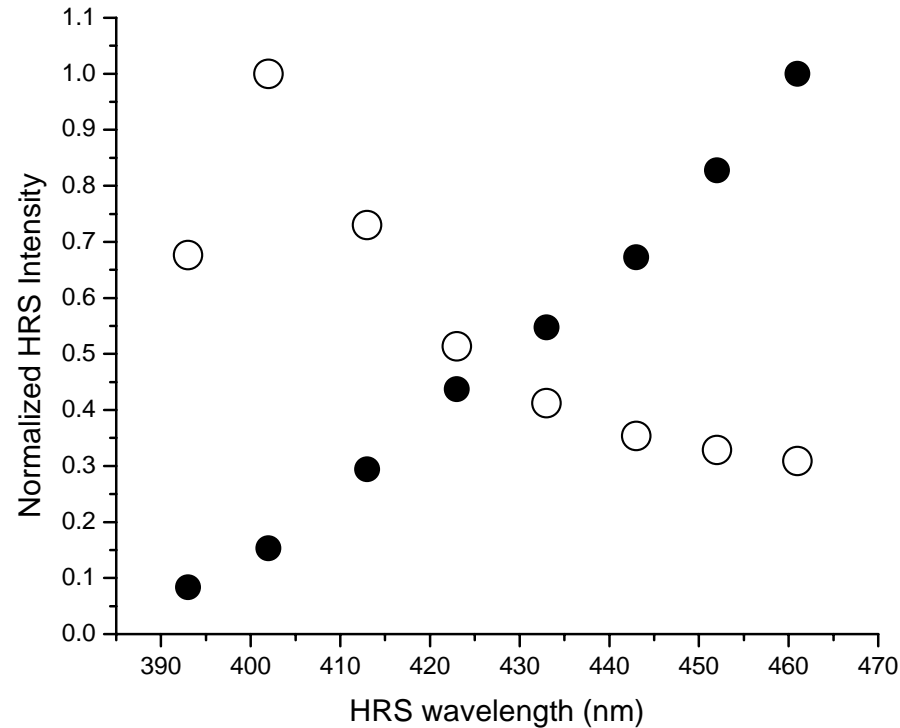
Addition of polymer, PVP stabilizes the **SH** signal

Excitation wavelength dependence of **SH** & **luminescence** of polymer stabilized NH_4Cl induced aggregates



- **SH** intensities increase by ~ two orders of magnitude
- The **luminescence** however, remains more or less similar

Wavelength dependent SH intensity profile



- Non-aggregated AgNPs resembles closely to their extinction spectra
- For aggregates, the SH intensity increases steadily with no apparent hint of a nearby maximum

Acknowledgement

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Thank you